

Submitted:
23.04.2019
Accepted:
27.08.2019
Published:
30.09.2019

Inter-rater reliability of an ultrasound protocol to evaluate the anterolateral ligament of the knee

Michel Kandel¹, Erik Cattrysse², Michel De Maeseneer³, Leon Lenchik⁴,
Marc Paantjens⁵, Marco Leeuw⁵

¹ Physical Therapy Practice, Oberriet, Switzerland

² Department of Experimental Anatomy, Vrije Universiteit Brussel, Brussels, Belgium

³ Department of Radiology, Universitair Ziekenhuis Brussel, Brussels, Belgium

⁴ Department of Radiology, Wake Forest School of Medicine, Winston-Salem, NC, USA

⁵ Ministry of Defence, the Netherlands

Correspondence: Michel Kandel, Physical Therapy Practice, Staatsstrasse 46,
9463 Oberriet, Switzerland; e-mail: kandel.physio@bluewin.ch

DOI: 10.15557/JoU.2019.0027

Keywords

anterolateral
ligament,
musculoskeletal
ultrasound,
knee instability,
anterior cruciate
ligament,
knee

Abstract

Objectives: The aim of this study was to validate an ultrasound protocol for evaluating the anterolateral ligament of the knee. **Methods:** A Thiel technique cadaveric specimen was used to validate an optimal scanning position and develop an ultrasound protocol to evaluate the anterolateral ligament. Three musculoskeletal sonographers acquired short- and long-axis images of the anterolateral ligament in 36 knees from 18 healthy volunteers. Anterolateral ligament length, thickness, width, and distance between anterolateral ligament insertion and lateral tibia plateau were measured. Intraclass Correlation Coefficient (ICC) was calculated. **Results:** The inter-rater reliability for anterolateral ligament thickness was poor, ICC = 0.35 (95% CI: -0.06–0.63). The inter-rater reliability for anterolateral ligament length and width was good, ICC = 0.80 (95% CI 0.64–0.89), ICC = 0.88 (95% CI 0.79–0.94), respectively; and the inter-rater reliability for the distance between insertion and lateral tibia plateau was excellent, ICC = 0.96 (95% CI 0.93–0.98). **Conclusions:** Ultrasonography is a reliable method for evaluating the anterolateral ligament. There is an excellent reliability for the distal part of the anterolateral ligament. As injuries usually occur in this part of the ligament, this protocol may be used to evaluate the anterolateral ligament in patients with suspected anterior cruciate ligament tears in clinical practice.

Introduction

The publication of Claes *et al.*⁽¹⁾ in 2013 brought the anterolateral ligament (ALL) of the knee to the attention of researchers and clinicians. These authors investigated cadaveric knees based on the description of Paul Segond⁽²⁾, who saw a “pearly fibrous resistant band” associated with an avulsion fracture at the anterolateral proximal tibia (Segond fracture) in 1879. Claes *et al.* reported that 97% of 41 unpaired cadaveric knees had a well-defined ligamentous structure, which they designated the anterolateral ligament (ALL). Since then, the anatomical characteristics of the ALL have been further defined by many authors^(3–8). Among these, there is a consensus that the ALL is a triangular, anterolateral ligamentous structure, underneath the iliotibial band (ITB)⁽⁹⁾ (Fig. 1).

The function of this ligament is to provide anterolateral knee stability by preventing the lateral tibia from subluxation anteriorly relative to the femur^(9,10). Studies have

documented ALL injuries in 46% to 79% in combination with ACL injuries^(11,12). Persisting rotational instability after ACL reconstruction (prevalence 25%)⁽⁹⁾ seems to be due to insufficiency of these lateral structures⁽¹³⁾. Combined reconstruction of the ALL and ACL should be considered depending on patient history, clinical signs, imaging, and patient profile^(9,14).

Musculoskeletal ultrasonography (US) is a non-invasive, cost-effective, and valid method to visualize extra-articular structures in real time. Only a few studies investigated the visualization of the ALL with US^(15–19). These studies were unable to determine how to reliably visualize the ALL with US⁽²⁰⁾. It is hypothesized that point-of-care ultrasound (POCUS) of the ALL may be useful if an ACL tear is suspected. However, a standardized protocol in how to reliably visualize the ALL with US is needed.

The purpose of this study is to present a standardized protocol to visualize the ALL with US and to determine inter-rater reliability.

Materials and methods

Neri *et al.*⁽²¹⁾ reported that the maximum length of the ALL was reached in 30° flexion with internal rotation. More flexion resulted in a decrease in tension on the ALL. In order to be able to dynamically exam a patient’s knee without the help of an assistant, the patient can be placed in a lateral position. In this position the examiner is able to scan and control the position of the knee with more or less tension on the ALL by himself. To evaluate the use of US to visualize the ALL in this position, a Thiel embalmed cadaver specimen was used. A Thiel embalmed specimen was chosen due to its acoustic, mechanical, and elastic properties^(22,23). First, a dynamic ultrasound examination of the cadaveric knee was performed and images were stored on the ultrasound device (Fig. 2). Short and long axis images were acquired and measurements (length, width, thickness and distance between insertion and lateral tibia plateau) were performed by consensus. Following consensus by two experienced US examiners (Mdm, MK: MDM 20 years of experience, MK 5 years of experience) surgical needles were placed at the origin and insertion of the ALL. Second, the knee was dissected to evaluate the position of the needles. The ALL could be identified between the needles, as it ran slightly proximal and posterior from the lateral femur condyle over the lateral collateral ligament, attached to the lateral meniscus and then to the tibia, halfway between Gerdy’s tubercle and the fibula head (Fig. 3).

To consider a target population at risk, healthy active people between 18 and 55 years were included, by non-probability sampling. Informed consent was obtained from each participant, and the rights of human subjects were protected. Three raters, all physical therapists, MSc, with at least 3 years of experience in US (MAP,

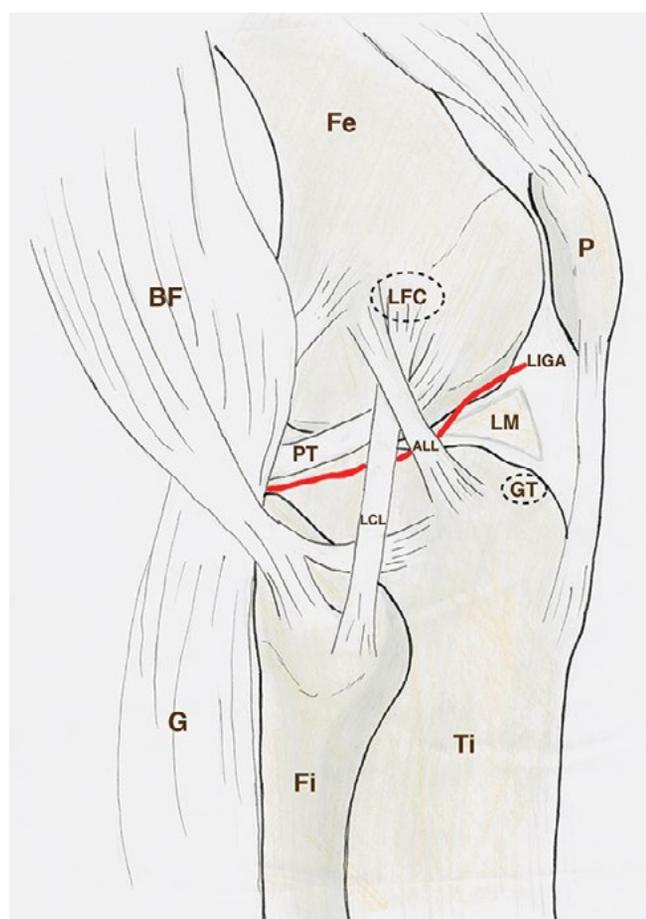


Fig. 1. Schematic drawing of the lateral side of the knee, deep to the iliotibial band. Fe, femur; Ti, tibia; Fi, fibula; P, patella; G, lateral head of gastrocnemius; BF, biceps femoris; LFC, lateral femur condyle; GT, Gerdy’s tubercle; PT, popliteus tendon; LCL, lateral collateral ligament; ALL, anterolateral ligament; LM, lateral meniscus; LIGA, lateral inferior genicular artery

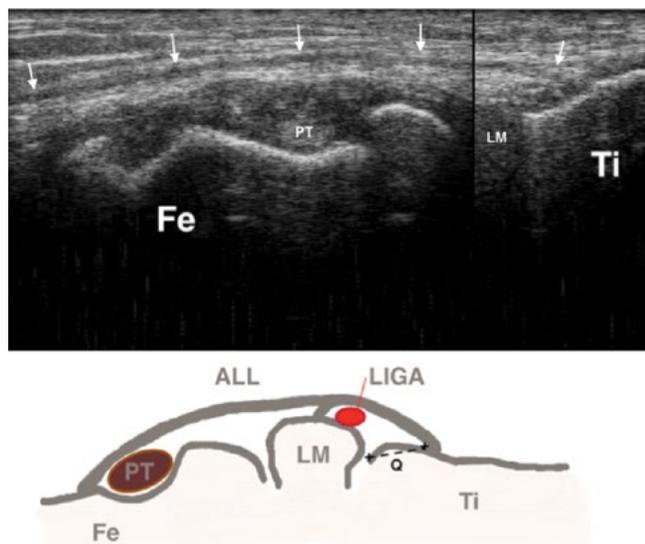


Fig. 2. Ultrasound image of the cadaveric knee showing the anterolateral ligament (arrows) attached to the tibia (Ti) running over the popliteus tendon (PT) to the femur (Fe) condyle. Schematic drawing of the structures (B): Fe, femur; Ti, tibia; LM, lateral meniscus; arrows, anterolateral ligament; LIGA, lateral inferior genicular artery; Q, measurement distance between anterolateral ligament insertion and tibia plateau

ML, MK) performed all measurements. Each sonographer completed a 4 hour training session in order to get familiar with the ALL protocol prior to this study. The volunteer underwent a clinical examination by an experienced physical therapist to exclude clinical anterolateral instability.

To visualize the ALL in vivo a standardized protocol based on the validation of the scanning position was defined with the participant lying on the ipsilateral side with the upper leg in 30° flexion and his foot hanging off the examination table. A pillow was placed under his

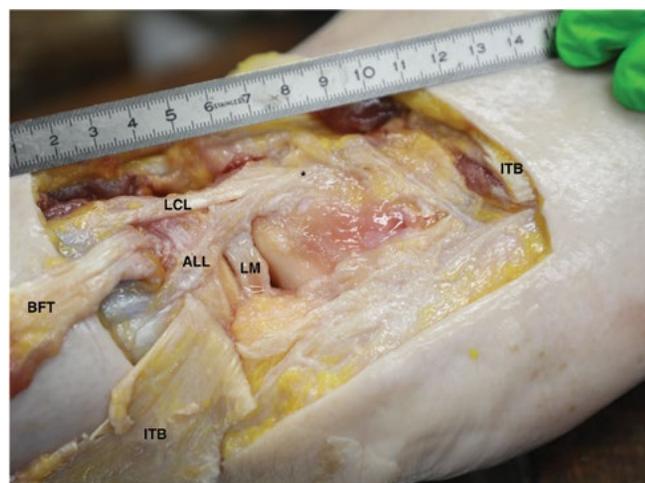


Fig. 3. Anatomical dissection of the lateral knee showing the anterolateral ligament (ALL), lateral femur condyle (*), lateral meniscus (LM), lateral collateral ligament (LCL) with the ilio-tibial band (ITB) and biceps femoris tendon (BFT) reflected

knee. The examiner sat behind the participant in order to easily adjust US settings and be able to flex and rotate the leg, if necessary. The ITB was located in its long axis at its insertion on Gerdy's tubercle. Then, the probe was slowly rotated towards the fibular head. Halfway between Gerdy's tubercle and head of the fibula, the distal insertion of the ALL can be found. In this position, the popliteus tendon and the lateral inferior genicular artery (LIGA) were used as landmarks to identify the ALL running to the lateral femur condyle. In this position (Fig. 4), length, thickness (just above the LIGA) and distance from insertion to tibia plateau were measured. The width of the ALL was measured in a short axis view above the LIGA. Images and measurements were recorded and stored on the US system.

For the three raters ($k = 3$) a good reliability was set at 0.75 (R_g), whereas a poor reliability was set below 0.5 (R_p)⁽²⁴⁾. The value of α is pre-specified to be 0.05 (which represents the probability of a Type I error). The power was set on 85% (Type II error), thus $\beta = 1 - 0.85 = 0.15$. Out of the equation, the minimal sample size required was $n = 26.7$ measurements.

The three raters performed measurements of the ALL with a Philips Affiniti 50G (Royal Philips, Amsterdam, The Netherlands) ultrasound device and an 18.5 MHz, linear 5 cm transducer on both legs of the participant.

Data analyses were performed using IBM SPSS Version 21 (SPSS Inc. Chicago, IL, USA). All data was checked for assumptions. Descriptive statistics were calculated, and the Intraclass Correlation Coefficient (ICC) was used to assess inter-rater reliability (ICC_{2,1}; two-way random effects model, single measurement type defined in absolute agreement) reported with 95% confidence interval (CI) of the estimated ICC. The level of reliability was based on the general guideline according to Koo, 2016⁽²⁵⁾.



Fig. 4. The participants were placed in a lateral position with the knee on a pillow in 30° flexion. The foot was hanging over the table. The positions of the probe are indicated by the red lines

Results

In the Thiel embalmed specimen the needle markings placed with US corresponded exactly to the ALL position observed at subsequent dissection and confirmed by an experienced anatomist (EC, 20 years of experience). Eighteen healthy subjects (12 male and 6 female) participated in this study. Mean (\pm standard deviation) of age, height, and weight were 41.2 (\pm 10.3) years, 179.2 (\pm 8.5) cm and 84.7 (\pm 13.1) kg. From 36 knees, two were excluded due to prior surgery. There were no signs of clinical anterolateral instability in the remaining 34 knees. The three raters were able to localize the ALL in 33 knees (97%). Characteristics of the participants and ALL are shown in Table 1. The ICC was calculated as the data was normally distributed. The inter-rater reliability of ALL thickness was poor, ICC = 0.35 (95% CI: -0.6-0.63). The inter-rater reliability was good for of ALL length and width, ICC 0.80 (95% CI: 0.64-0.89) and 0.88 (95% CI: 0.79-0.94), respectively; and excellent for the distance between insertion of the ALL and lateral tibia plateau, ICC 0.96 (95% CI: 0.93-0.98), as seen in Tab. 2.

Discussion

US has been used to visualize the ALL in five previous studies. Cianca *et al.*⁽¹⁶⁾ were the first to describe a short and long axis view of the ALL in a single knee of a healthy male subject. They reported that the ligament was easiest to identify when the knee was in 90° flexion with slight internal rotation. However, they had no anatomical correlation to prove that the visualized structure corresponded to the ALL. Cavaignac *et al.*⁽¹⁸⁾ reported a 100% sensitivity in visualizing the ALL in 18 unembalmed cadaveric knees by placing ultrasound guided metal needles in the proximal and distal ends of the ALL, using a 12-MHz linear transducer by a single radiologist. They concluded US to be a suitable tool to identify the ALL. In a technical note, the same authors described a supine scanning position with the knee in 90° flexion and internally rotated by an assistant in an operative setting⁽²⁶⁾. Capo *et al.*⁽¹⁵⁾ reported that US was not able to reliably identify the ALL at its femoral and tibial attachment sides and to distinguish it from the deep fibres of the ITB. They used a 14-MHz linear transducer and placed the knee in 30° to 60° flexion and internal rotation. Oshima *et al.*⁽¹⁷⁾ reported that US could be used to confirm the integrity of the ALL as they localized the ligament using real-time virtual sonography in 18 knees of 9 healthy male volunteers (28-37 years old). Thickness, length, and the distance between tibial insertion and the lateral tibial plateau were compared between MRI and US (in 30° knee flexion).

After evaluating US in a cadaveric observation, we determined the inter-rater reliability in 34 healthy knees. Mean length and width of the ALL in our study was 46.9 (\pm 4.2) mm, resp. 8.4 (\pm 2.3) mm, which corresponded well to with Neri *et al.*⁽²¹⁾. They reported ALL length of

Tab. 1. Descriptive statistics of participants (age, height, weight, BMI) and ALL measurements (length of ALL, thickness of ALL, width of ALL, distance to tibial plateau). All measurements are given in mm. ALL – anterolateral ligament

	n	Lower	Higher	Mean	SD
Age (year)	33	23	54	41.2	10.3
Height (cm)	33	164	188	179.2	8.5
Weight (kg)	33	63.3	104	84.7	13.1
BMI	33	21.5	31.1	26.3	2.9
ALL length	33	38.7	53.3	46.9	4.2
ALL thickness	33	0.52	1.24	0.94	0.16
ALL width	33	4.4	11.7	8.4	2.3
Distance to tibia plateau	33	2.2	9.2	5.7	1.8

45.29 (\pm 4.1) mm in 30° knee flexion and a width of 8.36 (\pm 0.69) mm in 84 fresh frozen cadaveric knees. Faruch *et al.*⁽¹⁹⁾ reported an ALL thickness of 0.97 (\pm 0.13) mm using US in 30 healthy subjects. Taneja *et al.*⁽²⁷⁾ reported a distance of 5.7 mm in MRI of 36 knees; Claes *et al.*⁽¹⁾ reported a mean distance of 6.5 (\pm 1.4) mm in 41 cadaveric knees.

In our study the Intraclass Correlation Coefficient (ICC) was poor for ALL thickness, good for ALL length and width and excellent for the distance between insertion and lateral tibia plateau. Our findings are consistent with prior studies^(3,17), that reported variability in the femoral attachment and a strong connection between the structures around the lateral femoral condyle, making the ALL more difficult to identify in this area. The poor consistency in the ALL thickness measurement may be due to the accuracy of US measuring beyond millimetres. A small measurement error of 0.1 mm, indicates a difference of 11% to the mean thickness (0.9 mm). Faruch *et al.*⁽¹⁹⁾ reported the difference between ALL thickness in healthy- (0.97 \pm 0.13 mm) and ALL injured subjects (1.46 \pm 0.27 mm) measured with US. This means an increase in ALL thickness of more than 50%. Due to the small standard deviation and despite a poor reliability it can be assumed that this protocol would be able to detect such an increase. The good ICC of the ALL width measurement indicates the possibility to reliably evaluate the ALL in short axis, between the ITB and the LCL around the joint line.

Tab. 2. Intraclass correlation coefficients for ALL length, thickness, width, and distance to tibia. Also shown 95% confidence interval and significance

	Intraclass correlation	95% confidence interval		Significance
		Lower bound	Upper bound	
ALL length	0.799	0.643	0.894	<0.001
ALL thickness	0.346	-0.058	0.0632	0.038
ALL width	0.884	0.794	0.939	<0.001
Distance to tibia plateau	0.959	0.927	0.978	<0.001

Nearly perfect reliability of the measurement of the distal insertion of the ALL has important implications for patient care. Almost all injuries of the ALL are located in the distal insertion of the ligament. Faruch *et al.*⁽¹⁹⁾ found that 100% of ALL injuries that occur in combination with ACL tears are located at the tibial attachment. Visualisation with US has the advantage of not only being able to show bony avulsion, the Segond fracture, but also show a pure ligamentous injury, which may lead to similar mechanical instability.

Our study has several limitations. Healthy active participants were included in our study. Our results may not hold up in patients suspected of having an ACL tear, where there might be pathological changes of the ALL. Integrity instead of morphologic characteristics should be evaluated in this situation. Studies in pathological cases are needed. Validation of the ultrasound protocol was done on a single Thiel embalmed cadaveric knee. The advantage of this embalming method is that the specimens retain tissue characteristic as in a fresh specimen in contradistinction to classic embalming where tissues harden and tissue planes become inseparable. Despite a good agreement between US and dissection, this can only be considered as a minimal validation. The mean age of the participants (41 years) did not entirely

match the mean age of people at risk for an ACL tear (18 to 25 years)⁽²⁸⁾.

Conclusion

The US protocol presented is reliable for evaluating the anterolateral ligament of the knee. There is an excellent reliability for the distal part of the ALL. As injuries typically occur in this part of the ligament, our protocol is promising for evaluating the ALL in patients with suspected ACL tears in clinical practice and on the playfield.

Conflict of interest

The authors declare that they have no conflict of interest.

Acknowledgment

We thank the Anatomical Research Training and Education (ARTE) of the Vrije Universiteit Brussel, Belgium to perform the cadaveric evaluation and the SOMT University, Amersfoort, the Netherlands for the use of the facilities and equipment in this study.

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